

Correlation between wall shear stress and wall rupture properties in ascending thoracic aortic aneurysms

Prof. Stéphane AVRIL

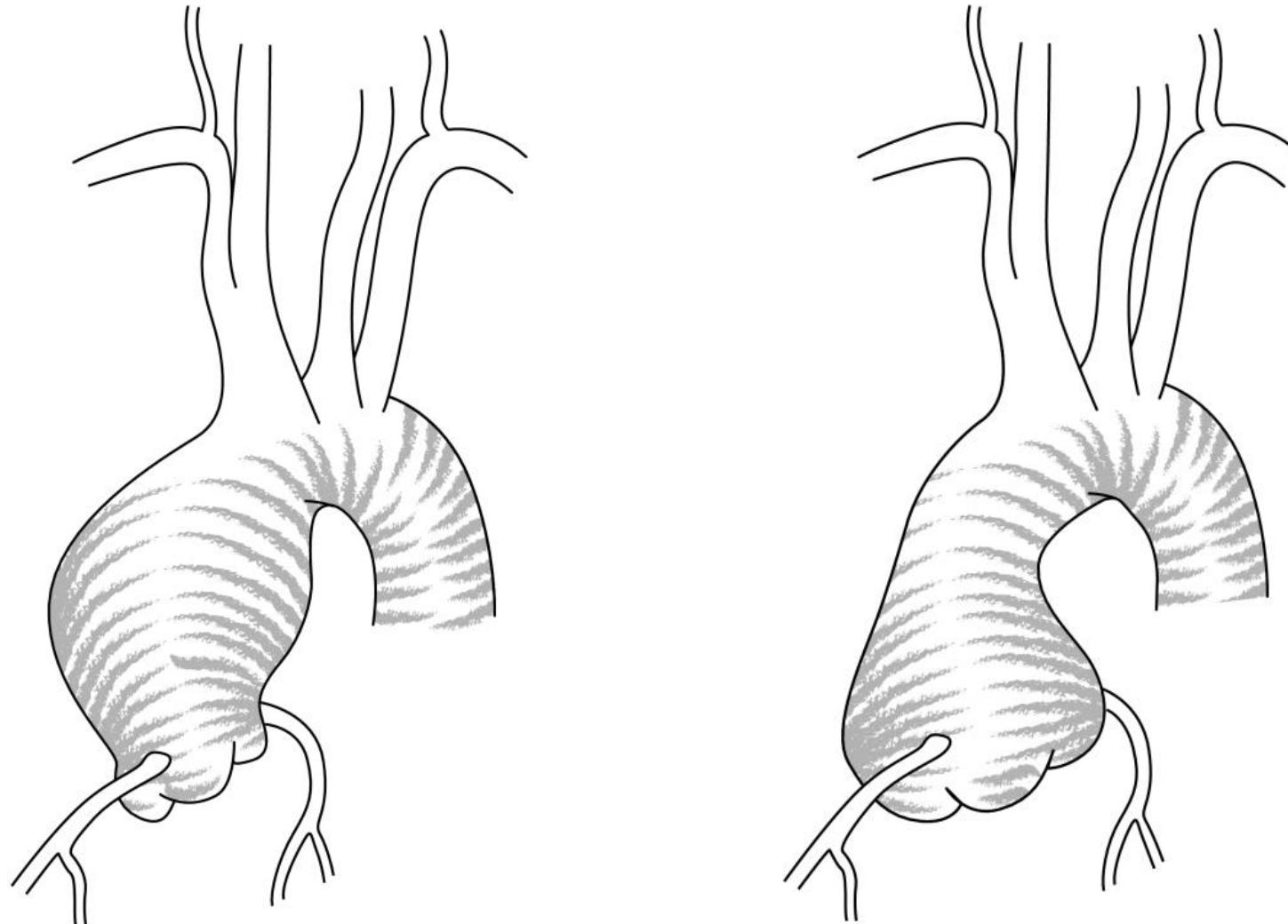


44^{ème} CONGRES
SOCIETE DE
BIOMECANIQUE |

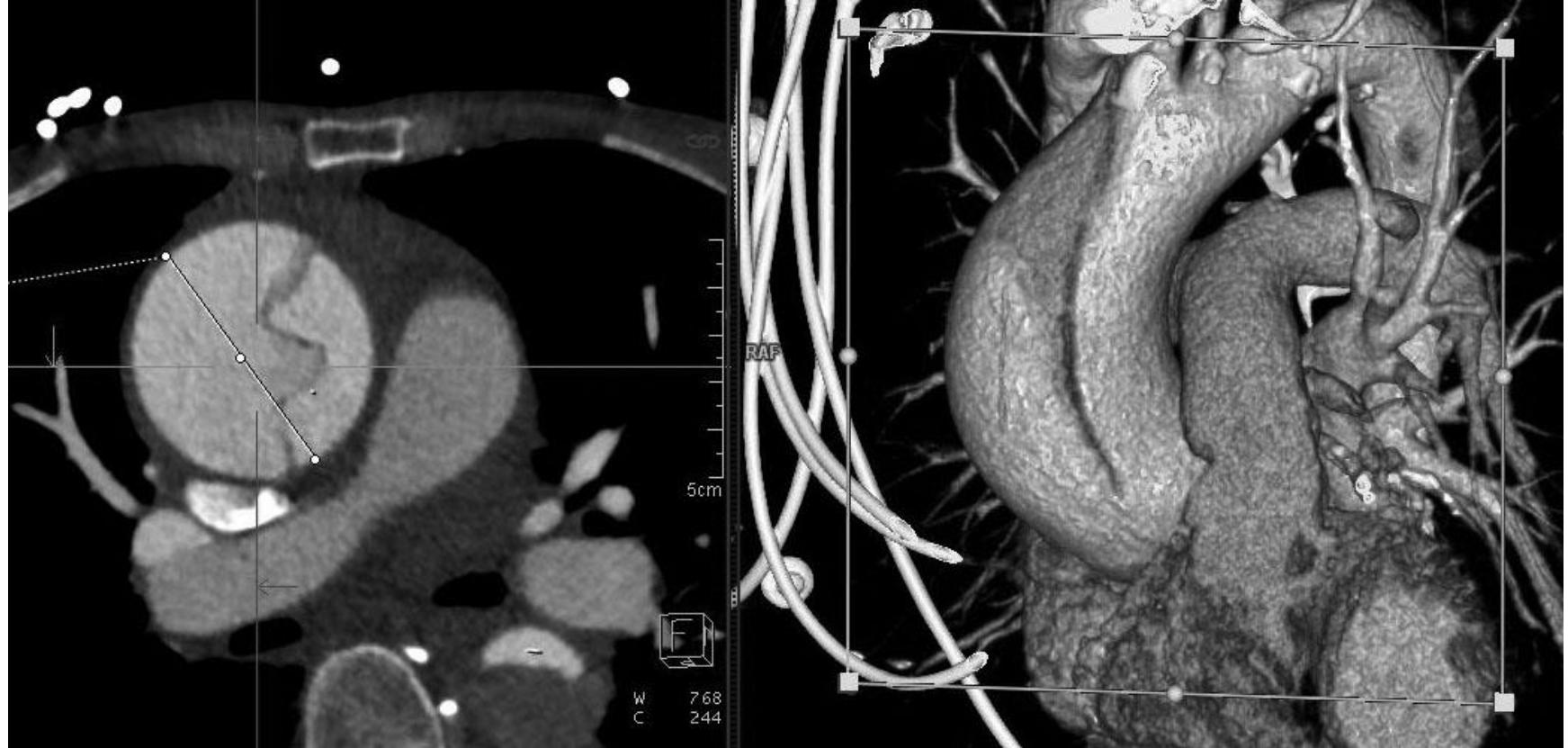
28 -30 Octobre 2019
Poitiers, France

@SB2019Poitiers

Aortic root dilatations and ascending thoracic aortic aneurysms (ATAA)



Risks: Aortic dissections



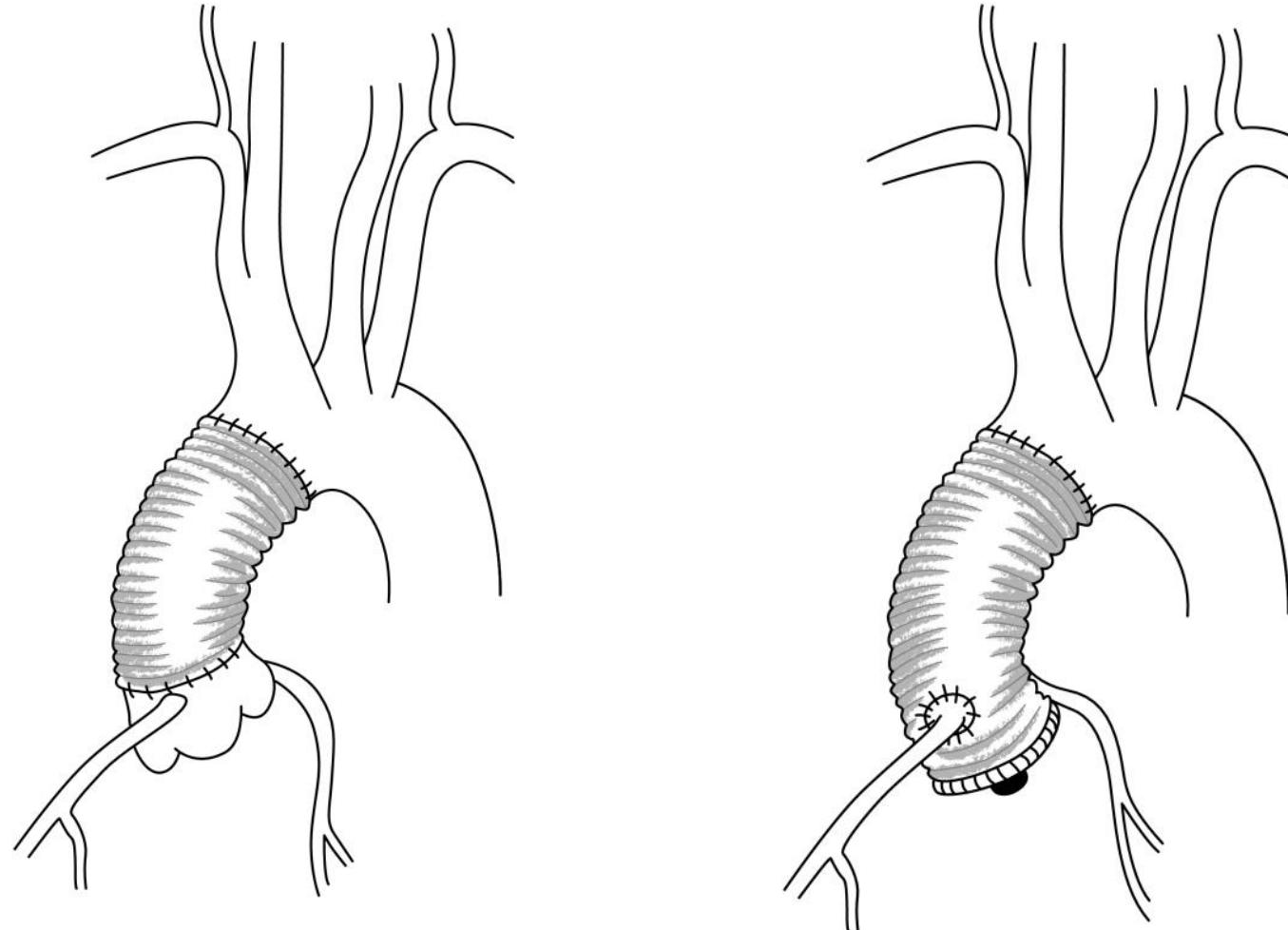
Surgical elective repair of ATAA

■ Indications:

- Aortic insufficiency requiring surgical correction
- Size ≥ 55 mm
- Size ≥ 50 mm in patients with Marfan syndrome or bicuspid valves
- Growth rate ≥ 1 cm/year

- More and more aneurysms are detected at an early stage (incidence >8% for males >65 years old).
- >90000 interventions per year in Europe and USA

Surgical techniques for ATAA repair

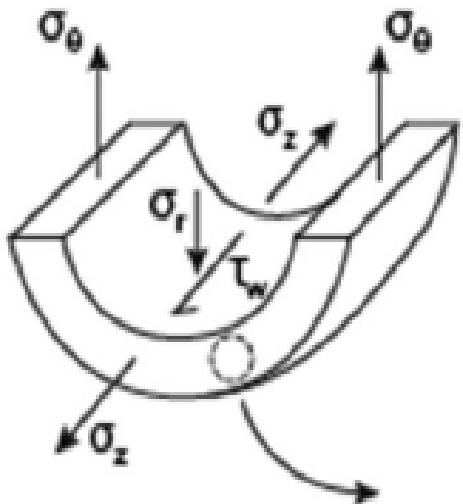


Current situation

- **Current indications:**
 - 25% ATAA < 5.5cm rupture : 15000 deaths**!
 - 60% of ATAA > 5.5 cm never experience rupture!
 - 9% mortality and morbidity after ATAA repair
- **In summary: inappropriate decisions and misprogrammed surgical interventions have major consequences!!**
- **Need insightful assistance from biomechanics ☺☺☺**

** Pape et al, *Aortic Diameter ≥5.5 cm Is Not a Good Predictor of Type A Aortic Dissection Observations From the International Registry of Acute Aortic Dissection (IRAD)*, Circulation, 2007

Basics of arterial mechanics

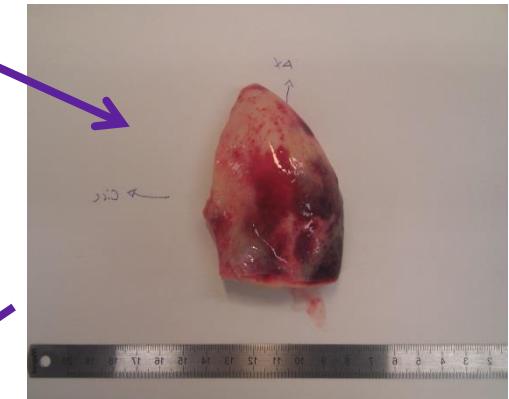
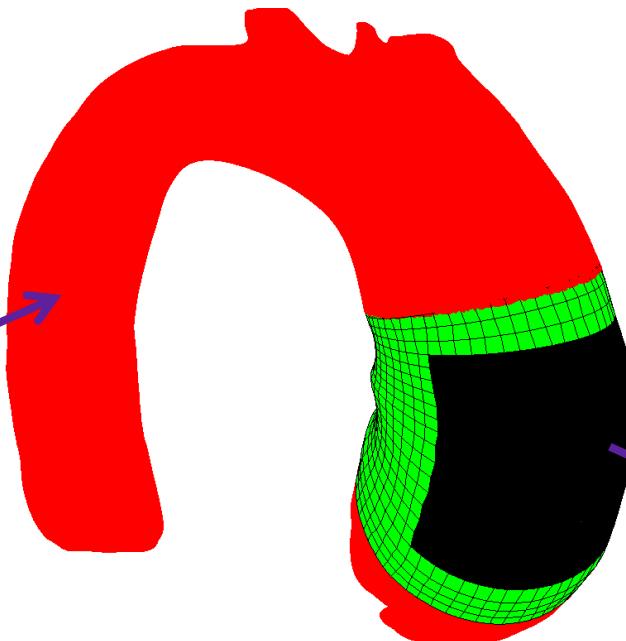
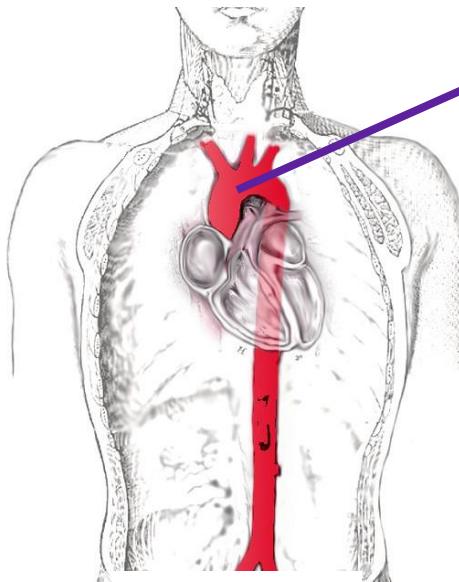


$$\tau_w = \frac{4\mu Q}{\pi a^3},$$

$$\sigma_\theta = \frac{P a}{h}$$

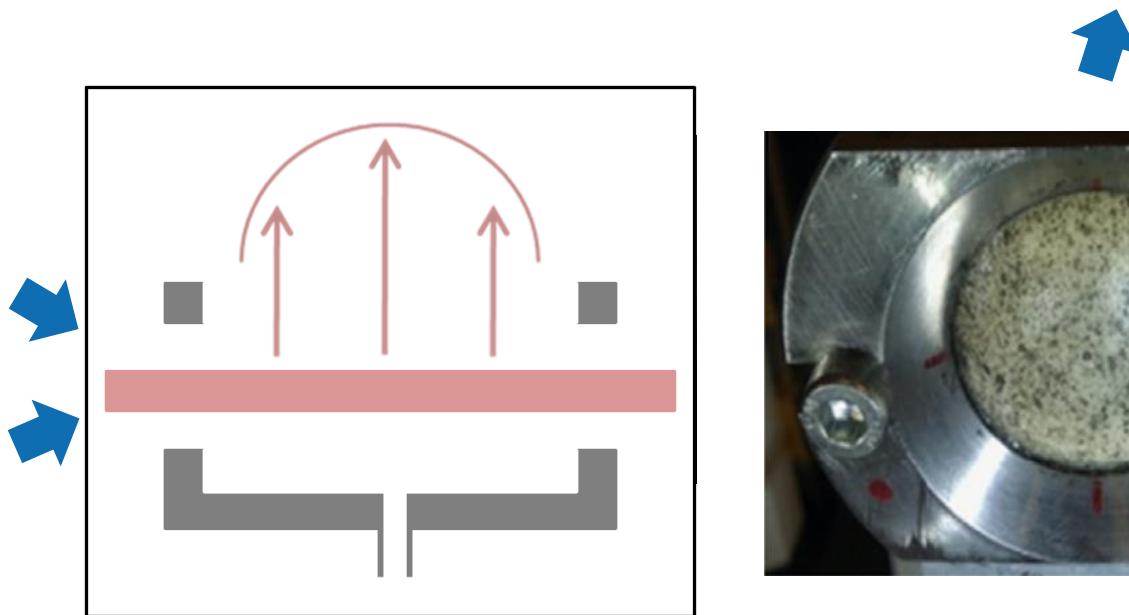
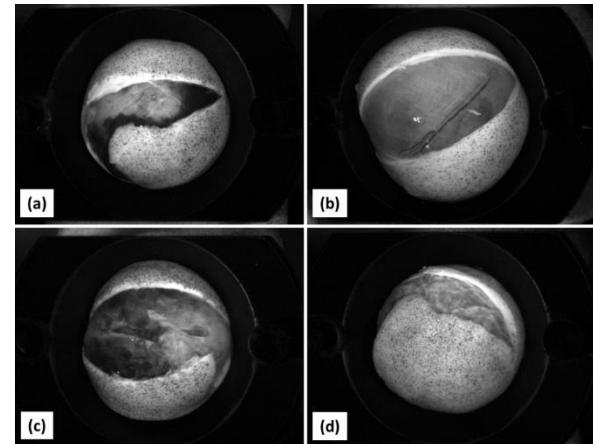
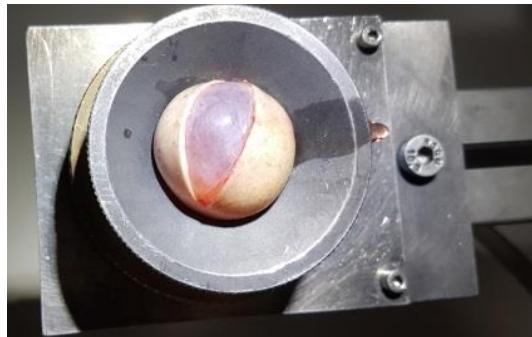
Humphrey JD (2002) *Cardiovascular Solid Mechanics: Cells, Tissues, and Organs*, Springer-Verlag, NY

Collection of the samples

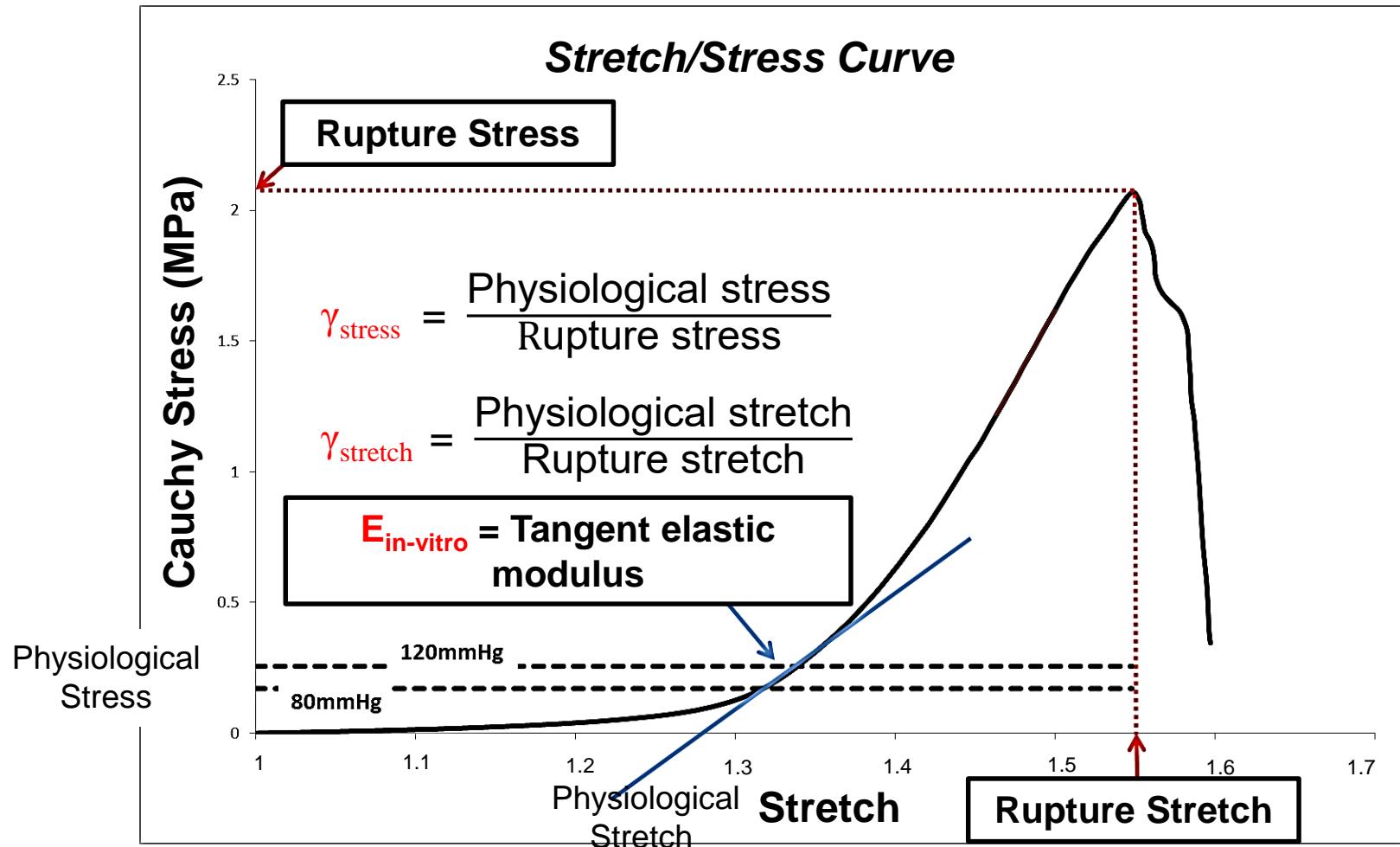


Bulge inflation test

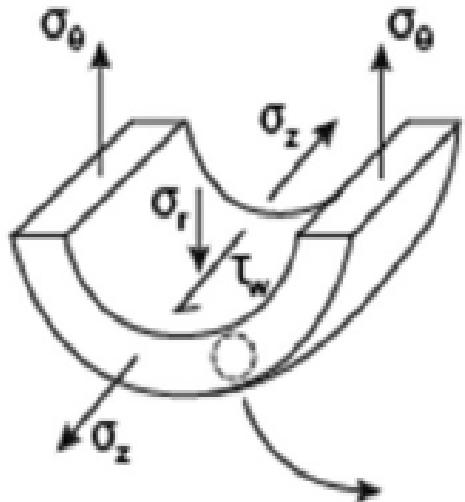
Romo et al. Journal of Biomechanics -
2014



Rupture risk estimation



Basics of arterial mechanics

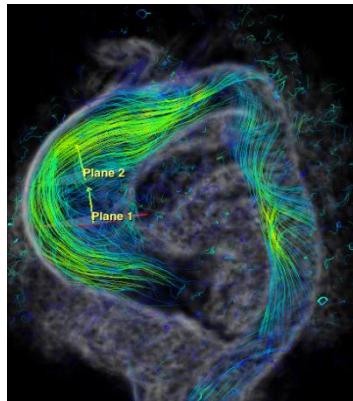


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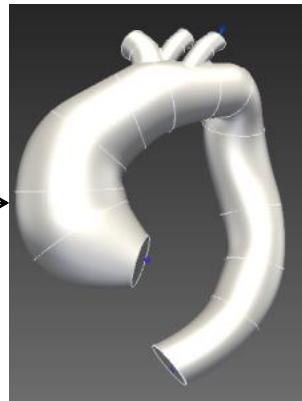
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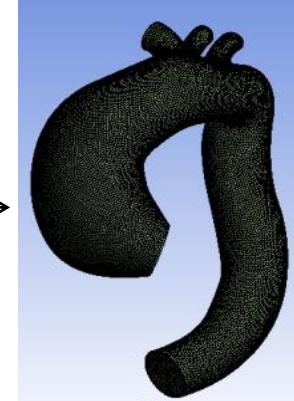
AORTIC HEMODYNAMICS ASSESSMENT



Preoperative dynamic imaging
4D MRI

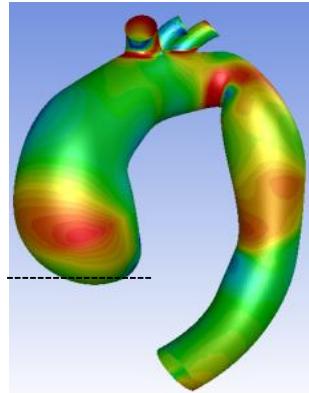


CAD

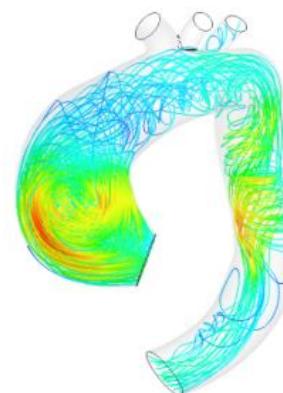


Mesh

Numerical
Solution



TAWSS

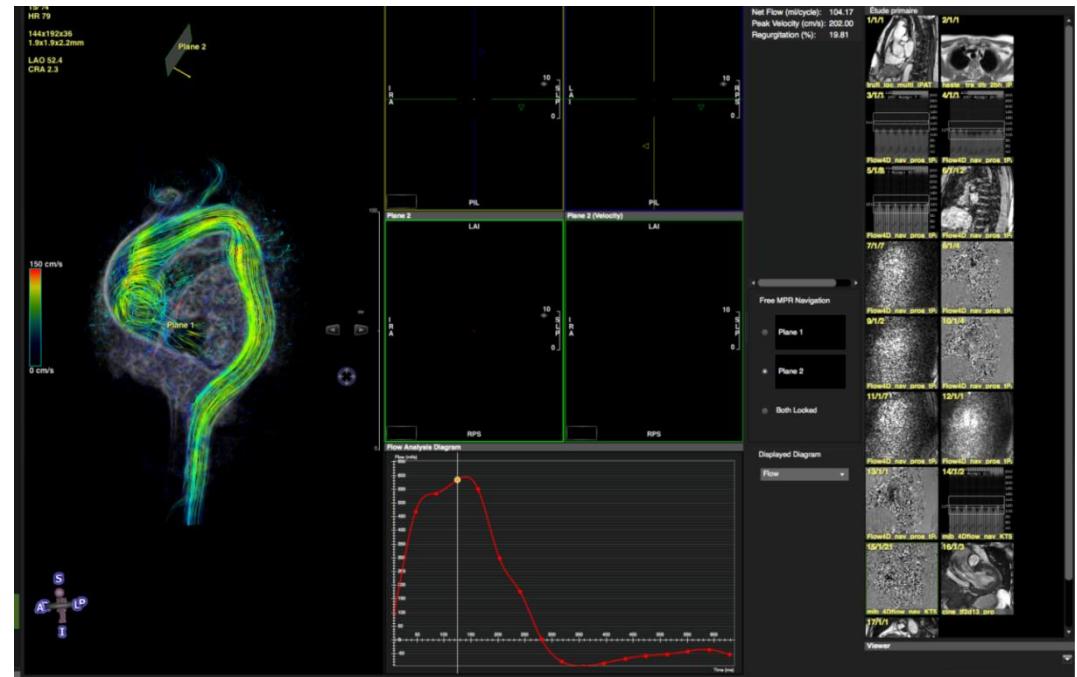


Streamlines, velocity

4D MRI images - Pre-processing

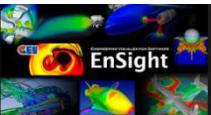
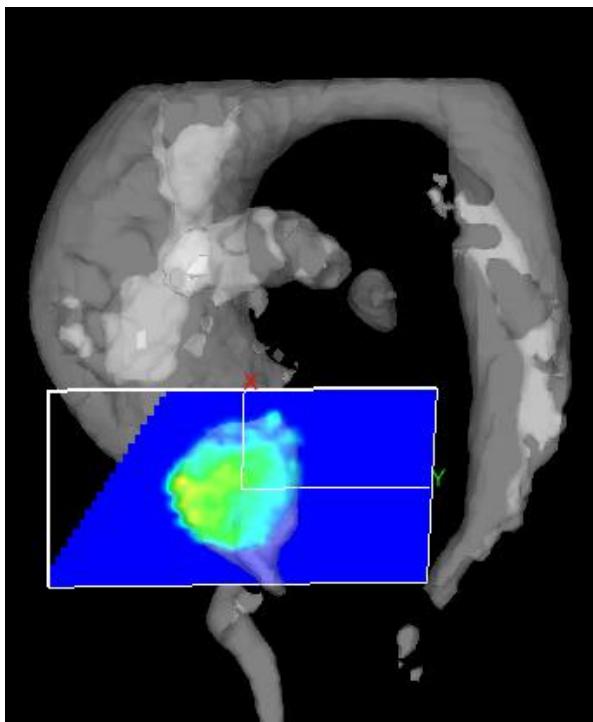


Siemens 3T Prisma



Patient Specific BCs - Velocity profile mapping

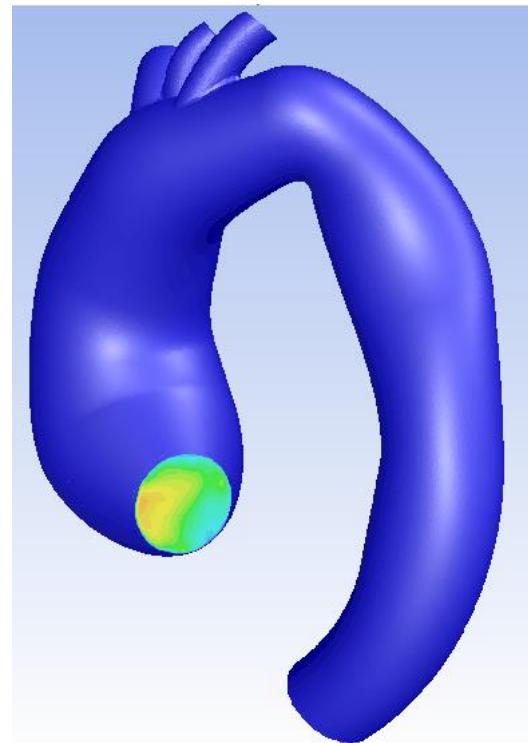
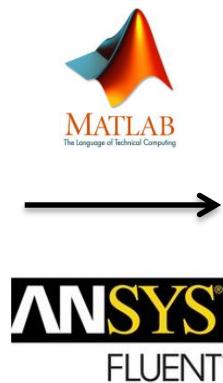
4D MRI data Velocity Profile



[4 m/s]

avril@emse.fr

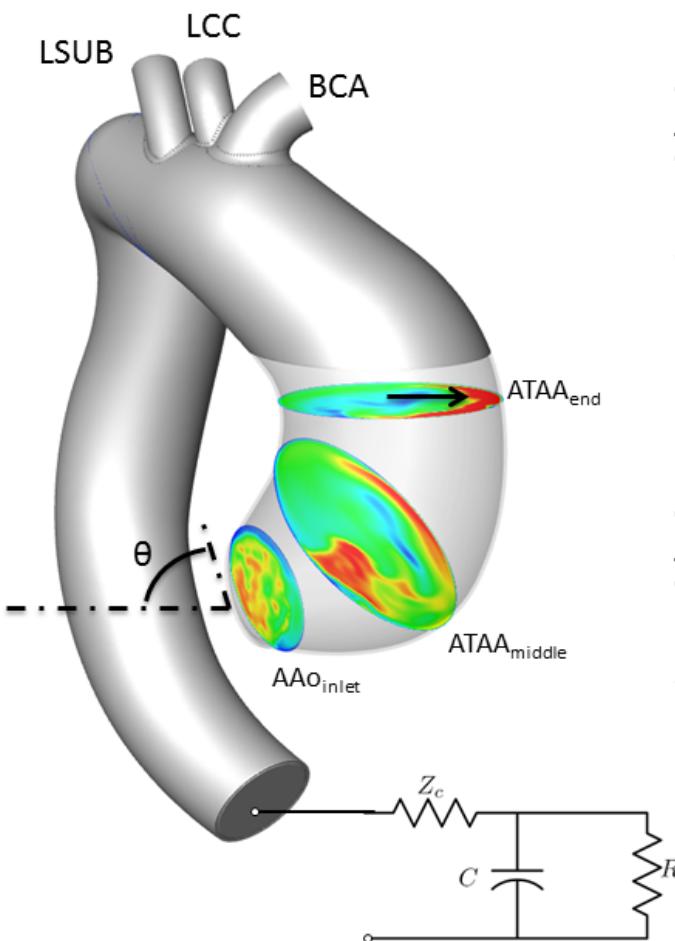
CFD Velocity Profile



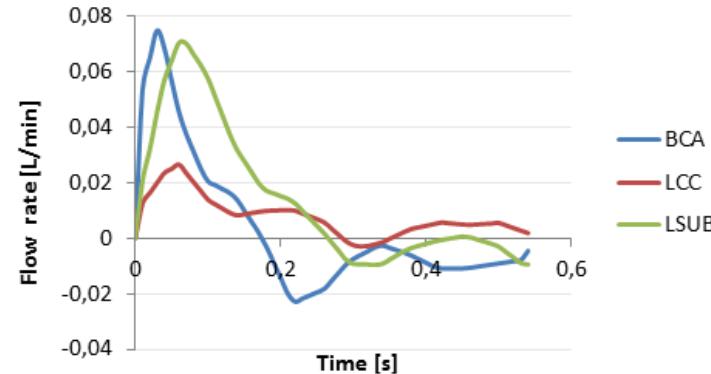
Stéphane Avril - 2019 Oct 29 - SB Poitiers

CFD - Numerical resolution

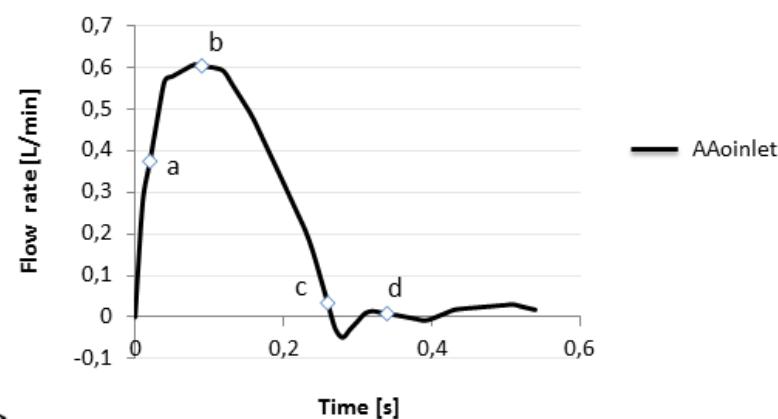
A



B



C



Hemodynamics indices

Time averaged wall shear stress (WSS):

$$TAWSS = \frac{1}{T} \int_0^T WSS \, dt$$



Oscillatory Shear Index:

$$OSI = 0.5 \left[1 - \left(\frac{\left| \int_0^T WSS(s, t) \cdot dt \right|}{\int_0^T |WSS(s, t)| \cdot dt} \right) \right]$$

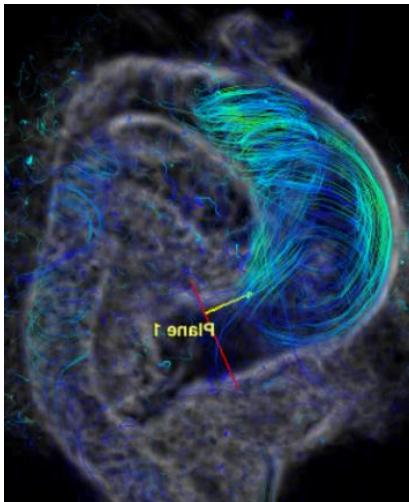
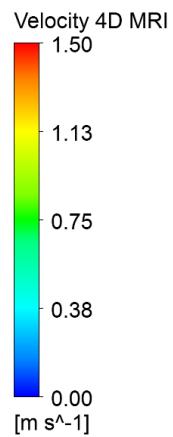
where T is the period of the cardiac cycle and WSS is the instantaneous wall shear stress.

Morbiducci, U., R. Ponzini, G. Rizzo, M. Cadioli, A. Esposito, F.M. Montevercchi, A. Redaelli. Mechanistic insight into the physiological relevance of helical blood flow in the human aorta: an in vivo study. Biomech. Model. Mechanobiol. 10:339–355, 2011.

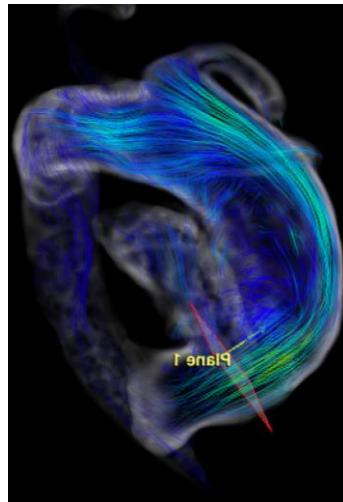
Velocity profiles



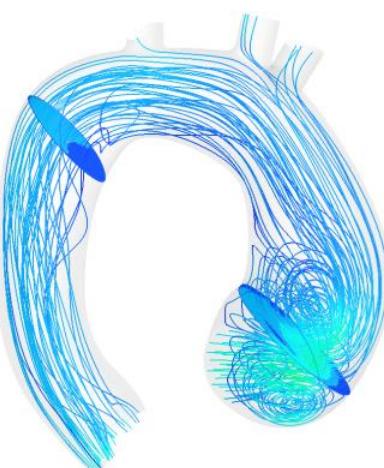
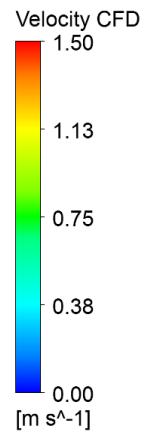
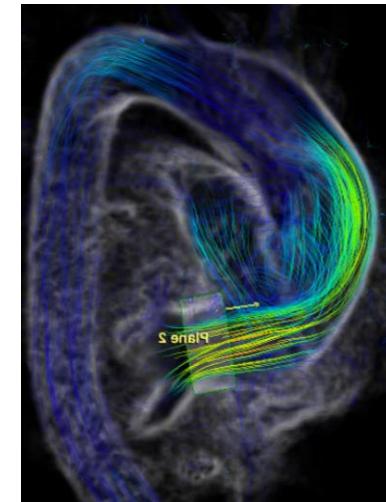
Patient 1 (BAV)



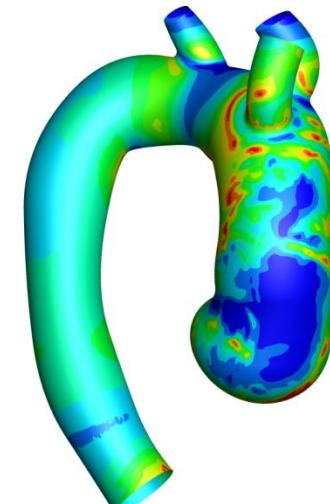
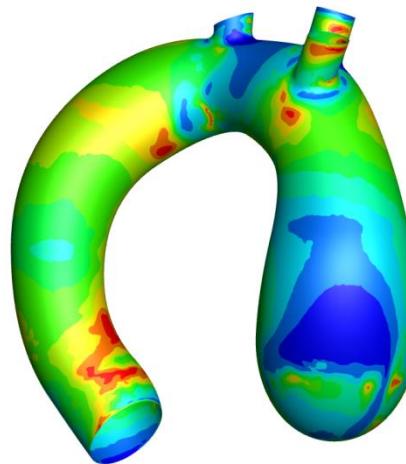
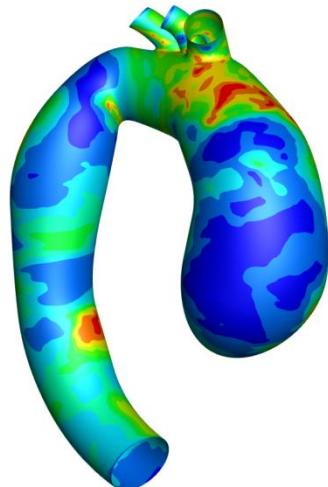
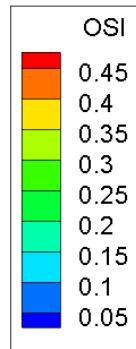
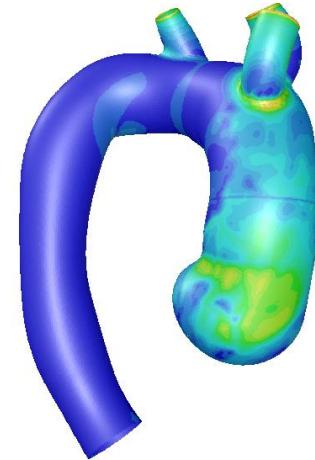
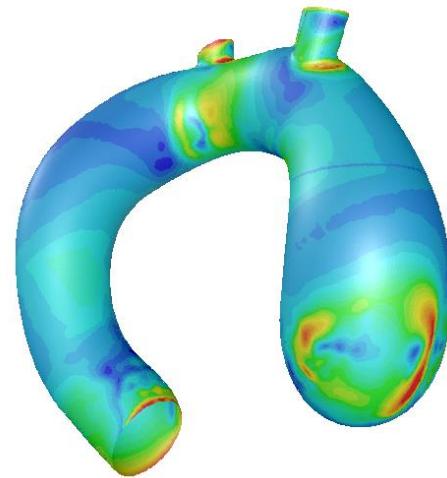
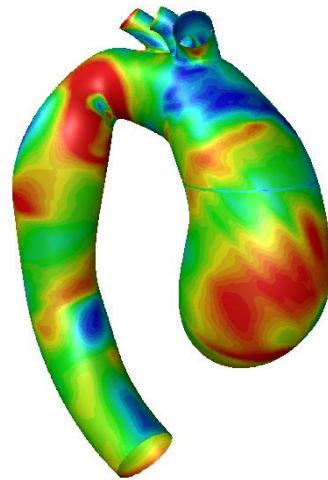
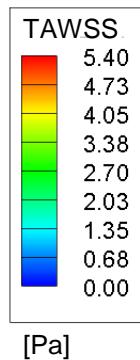
Patient 2 (TAV)



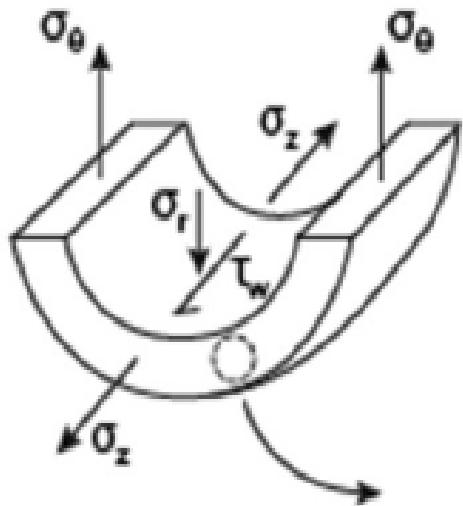
Patient 3 (BAV)



OSI and TAWSS



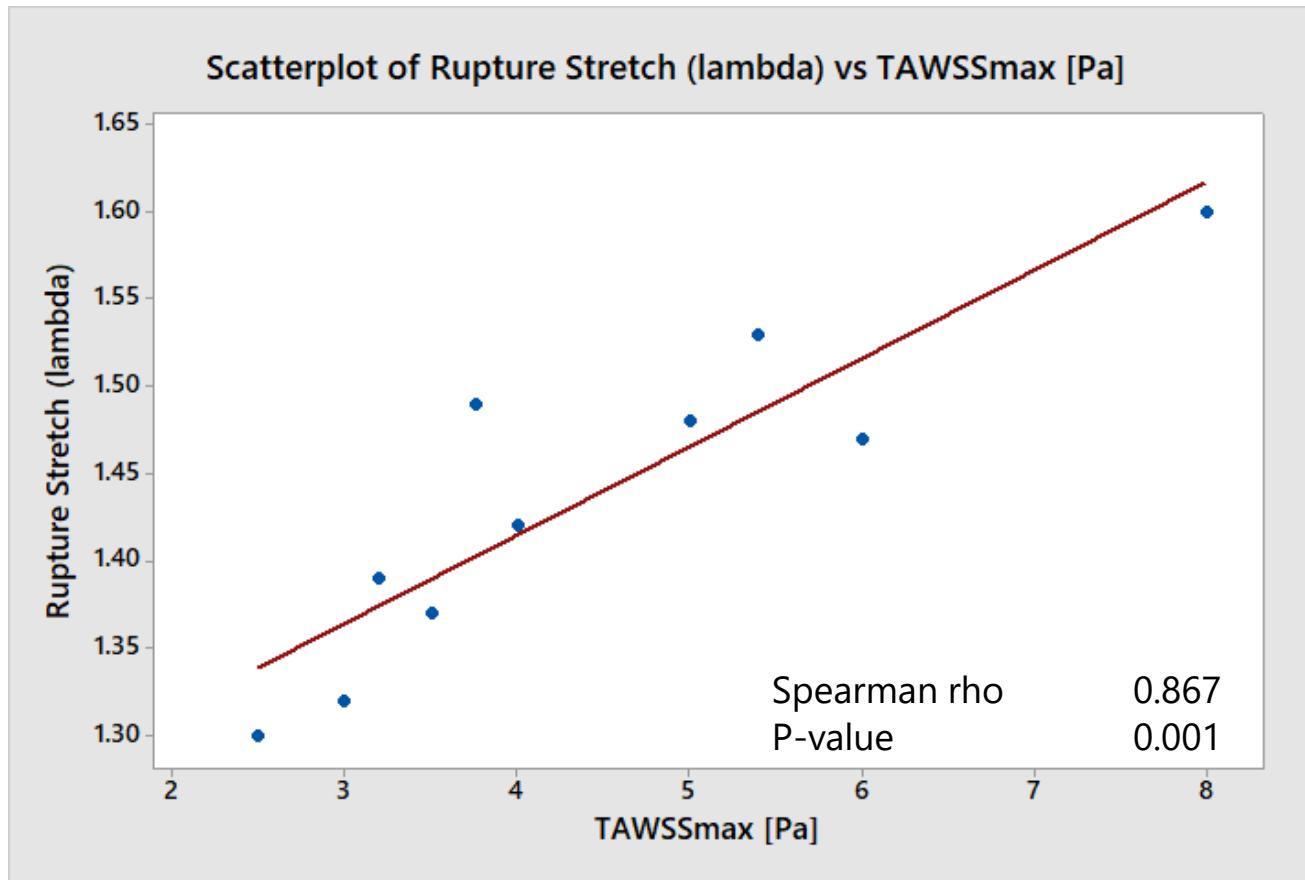
Basics of arterial mechanics



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Humphrey JD (2002) *Cardiovascular Solid Mechanics: Cells, Tissues, and Organs*, Springer-Verlag, NY

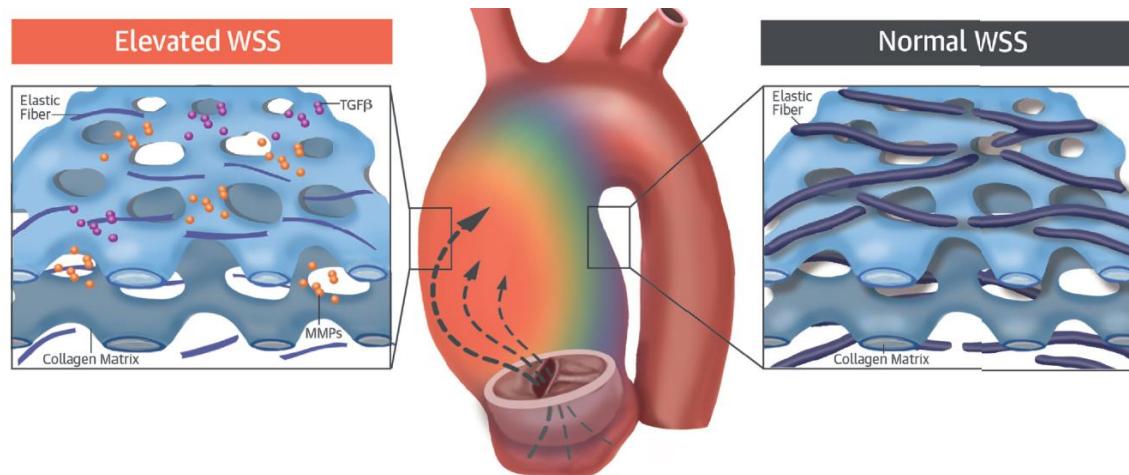
Statistical Analysis-Spearman Rho: λ_{rupture} vs. TAWSSmax [Pa]



Conde mi et al, IEEE Transactions on Biomedical Engineering, 2019

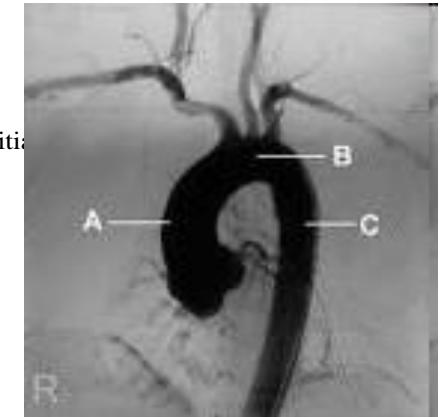
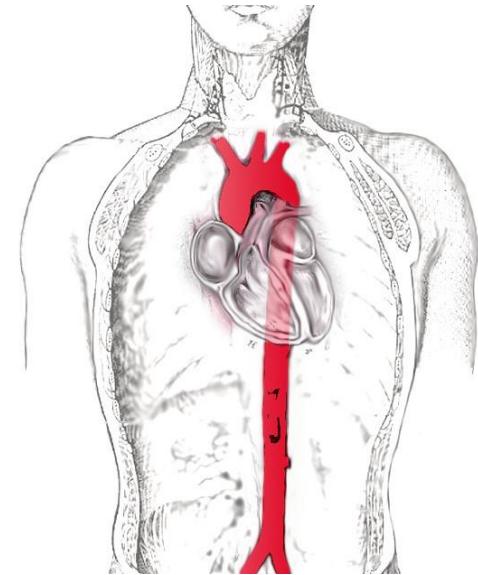
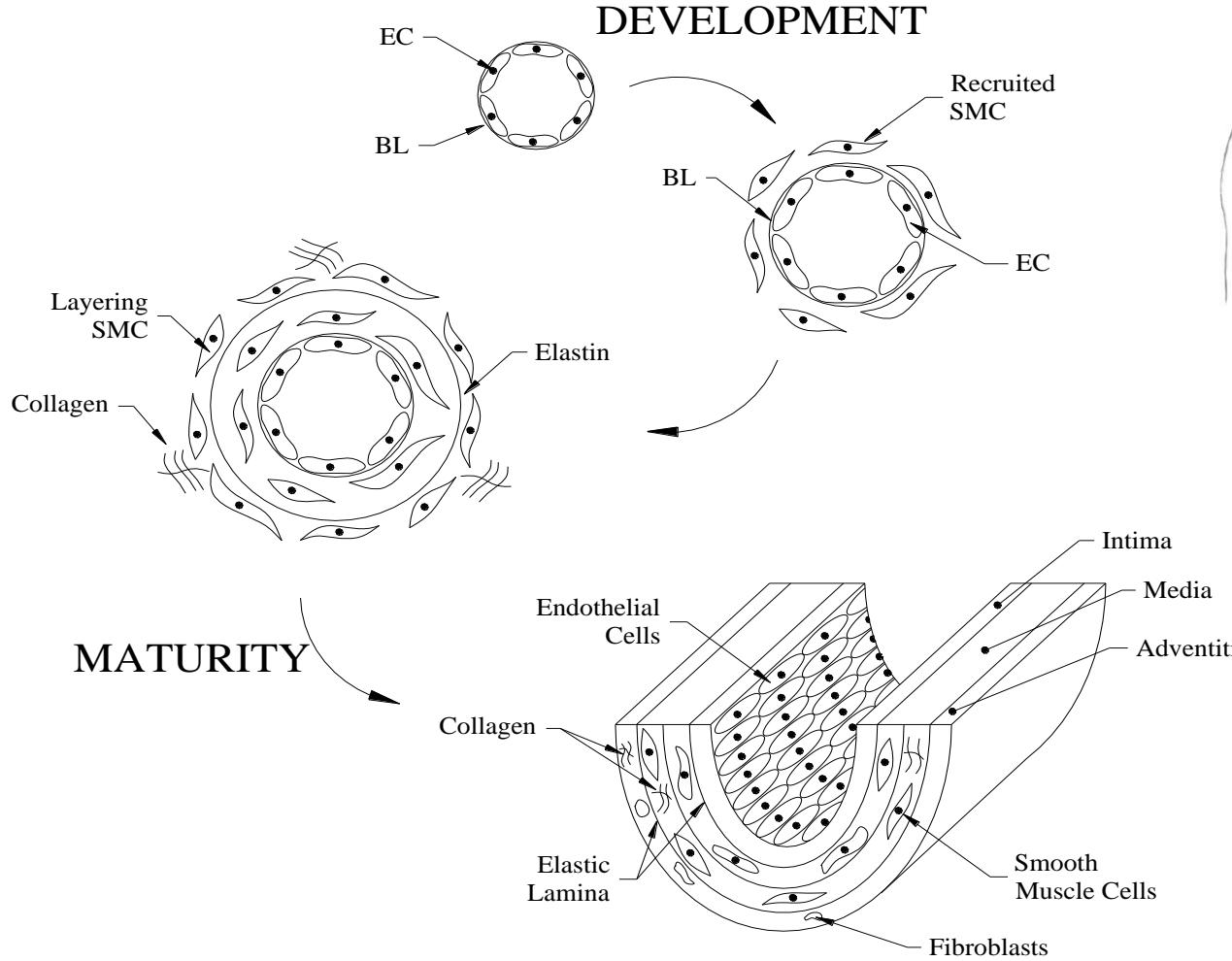
DISCUSSION

- Protective role of larger TAWSS, associated with low oscillatory wall shear stress?
- Controversial effects



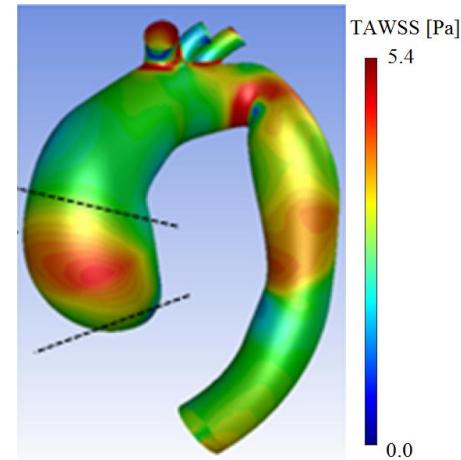
Guzzardi et al. JACC 2015

Modeling of mechanobiological processes



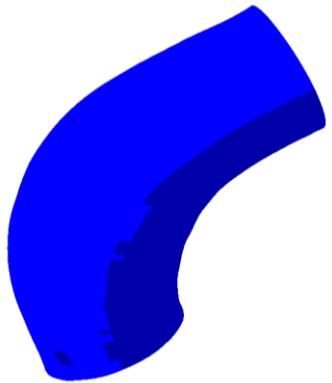
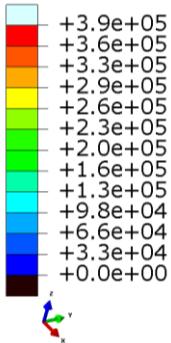
Patient-specific predictions

Growth and remodeling of a two-layer patient-specific human ATAA due to elastin loss

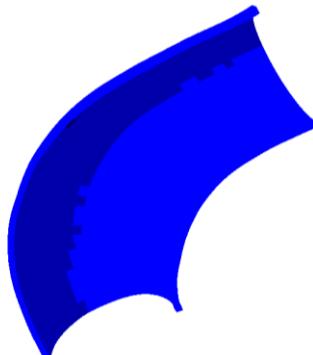
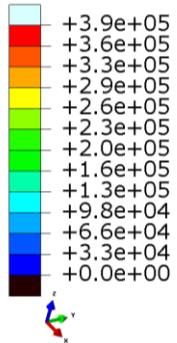


Small growth parameter

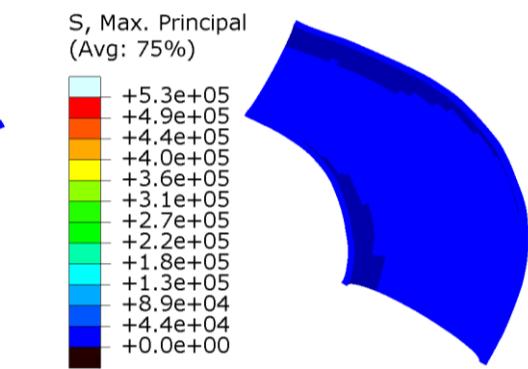
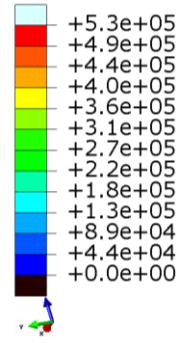
S, Max. Principal
(Avg: 75%)



S, Max. Principal
(Avg: 75%)



S, Max. Principal
(Avg: 75%)



Maximum Principal stress

Mousavi et al, BMMB 2019

avril@emse.fr



SUMMARY

- ATAA at higher “biomechanical” risk have an increased stiffness and a disturbed flow with reduced maximum TAWSS
- Our future work will focus on idiopathic ATAA and try to understand better what are the main triggers for the overstiffening.

Acknowledgements

- Olfa Trabelsi
- Aaron Romo
- Jin Kim
- Pierre Badel
- Frances Davis
- Victor Acosta
- Jamal Mousavi
- Solmaz Farzeneh
- Francesca Condemi
- Cristina Cavinato
- Jérôme Molimard
- Baptiste Pierrat
- Joan Laubrie
- Claudie Petit

- Ambroise Duprey
- Jean-Pierre Favre
- Jean-Noël Albertini
- Salvatore Campisi
- Magalie Viallon
- Pierre Croisille

- Chiara Bellini
- Matthew Bersi
- Jay Humphrey
- Katia Genovese



Funding:
ERC-2014-CoG BIOLOCHANICS



European Research Council
Established by the European Commission
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